Bouncing the Network: A Dynamical Systems Model of Auditory-Vestibular Interactions Underlying Infants' Perception of Musical Rhythm

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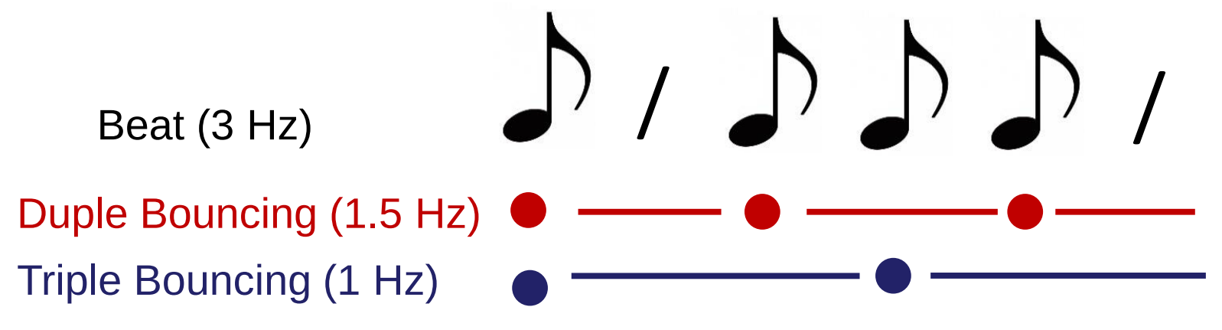
Background

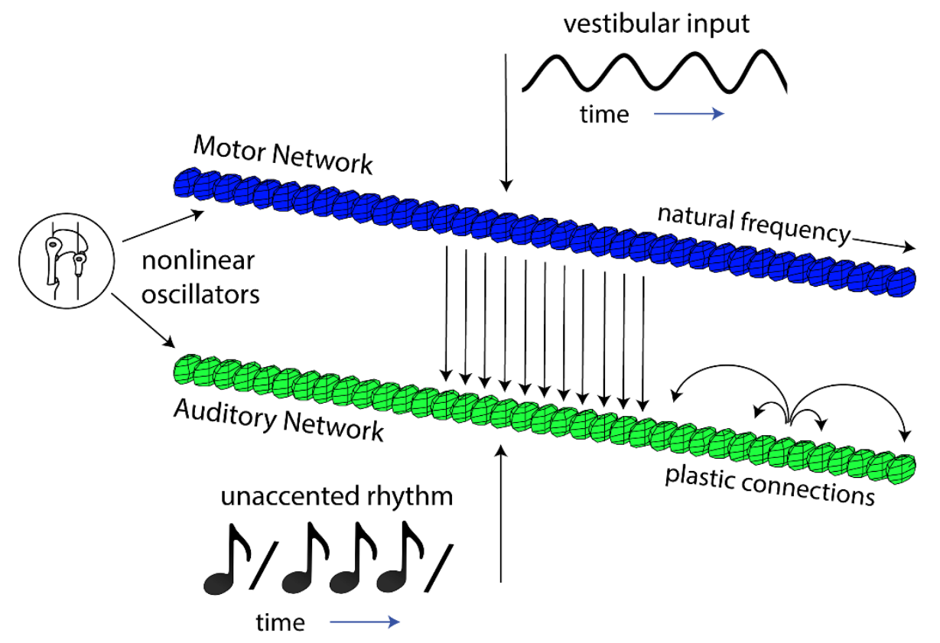
Previous work suggests that auditory-vestibular interactions, which emerge during bodily movement to music, can influence the perception of musical structure, such as the perception of accented beats in musical rhythm[1-3]. In a seminal study on the development of musical rhythm, Phillips-Silver & Trainor (2005) found that periodic, maternal bouncing of 7-month-old infants to an unaccented rhythm influenced infants' listening preferences for accented rhythms that matched the rate of maternal bouncing, suggesting that auditory-vestibular interactions shape rhythm perception in infancy. Expanding a recent theoretical model of infant rhythm perception[4], in the current study, we propose a dynamical systems model of auditory-vestibular interactions thought to underlie infants' listening preferences for accented rhythms. The model, featuring two neural networks of non-linear oscillators to represent developmentally nascent auditory and motor systems, was used to simulate the effect of maternal bouncing (e.g., vestibular input) on infants' listening preferences for duple- and triple-accented rhythms. First, we demonstrate that simultaneous auditory-vestibular training shaped the model's response to musical rhythm online, enhancing vestibular-related frequencies in the model's oscillatory activity. Next, we demonstrate that simultaneous auditory-vestibular training, relative to models that received auditory- or vestibular-only training, facilitated neural plasticity, producing stronger connections between network oscillators during a period of unsupervised learning. Finally, we show that models which received simultaneous auditory-vestibular training, but not models that received auditory-only or vestibular-only training, "preferred" rhythmic frequencies related to their "bouncing," resonating more strongly at frequencies related to the combined auditory-vestibular stimulation. This finding is qualitatively similar to infants' preferences for accented rhythms that matched the rate of maternal bouncing to an unaccented rhythm.



Phillips-Silver & Trainor, 2005

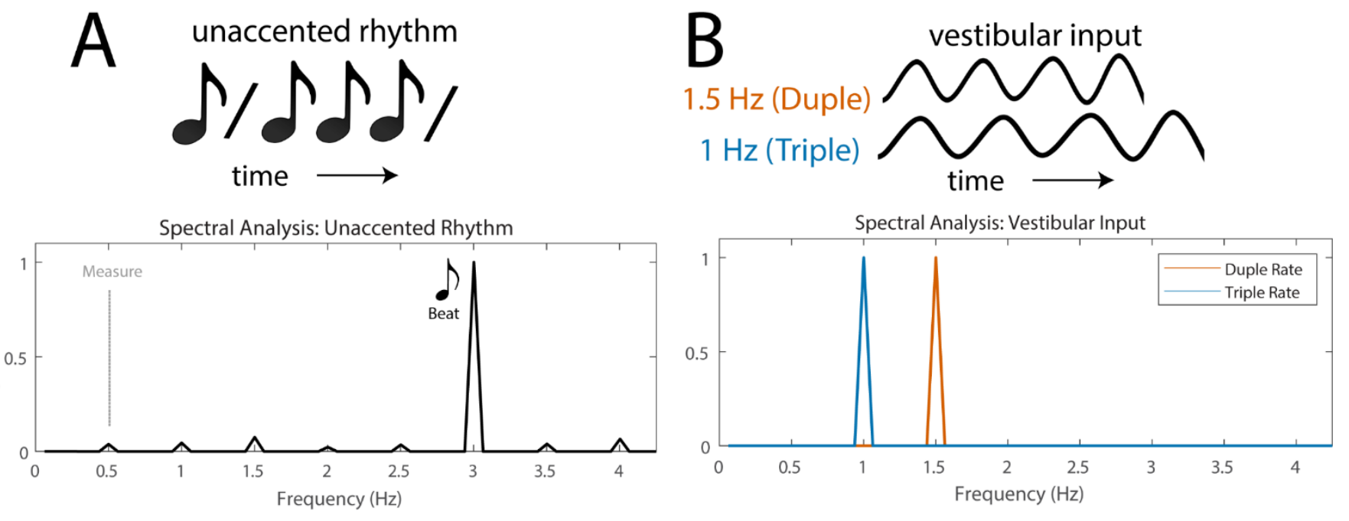
Methods

Model Architecture



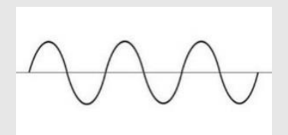
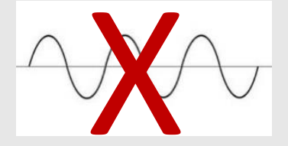
- The model consisted of two multi-frequency oscillatory neural networks, representing developmentally nascent auditory and motor systems, with a Hebbian plasticity rule in the auditory network.

Training Stimuli



- Notation and frequency-domain representations of the (A) Unaccented Rhythm (i.e., auditory input) (B) and Duple- and Triple-Rate Maternal Bouncing (i.e., vestibular input modeled as sinusoidal forcing).

Training and Test Procedures

Network	Training Phase	Test Phase
Auditory Network		
Motor Network		

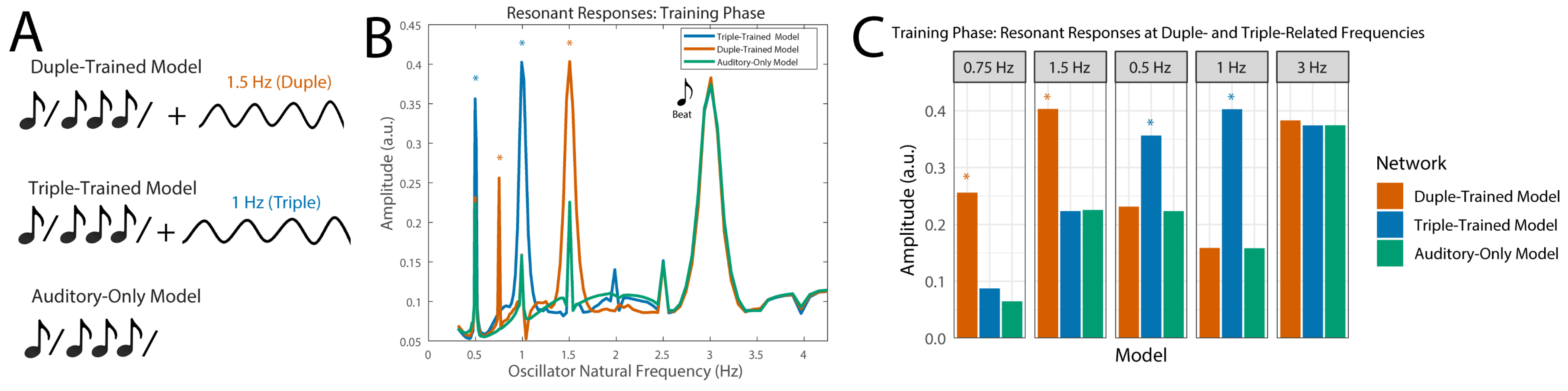
- Similar to the infants in Phillip-Silver & Trainor (2005), the model was trained on the unaccented rhythm (i.e., auditory input) and maternal bouncing at a duple or triple rate (i.e., vestibular input modeled as sinusoidal forcing).
- The model was, then, tested only on the unaccented rhythm to ascertain whether the model preferred rhythmic frequencies related to its bouncing.

Training Regimes

Model: Training	Auditory Training	Vestibular Training
Duple-trained model	X	X
Triple-trained model	X	X
Auditory-only model	X	-
Duple-only model	-	X
Triple-only model	-	X

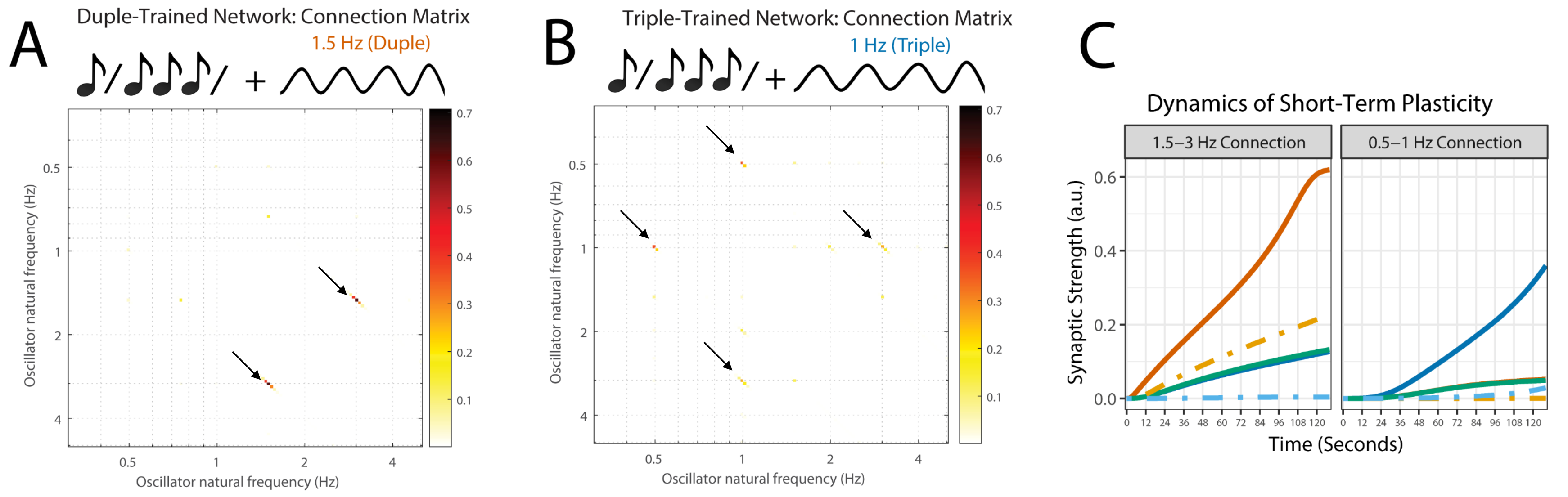
- To assess the effects of combined auditory-vestibular training on the model's behavior, two models were trained on simultaneous auditory-vestibular input (e.g., duple- and triple-trained models), similar to the infants in Phillips-Silver & Trainor (2005).
- To assess the independent effects of auditory or vestibular training on the model's behavior, three control models were trained on auditory-only input (e.g., auditory-only model) or vestibular-only input (e.g., duple- and triple-only models).

Vestibular Input Shapes the Neural Response to Musical Rhythm



(A) Training stimuli for the duple-trained, triple-trained, and auditory-only models. **(B)** Resonant responses in the auditory network of the duple-trained (red), triple-trained (blue), and auditory-only (green) models during the final half of the training procedure. **(C)** Resonant-response amplitude values that were extracted from the resonant responses in the duple-trained (red), triple-trained (blue), and auditory-only (green) models for duple-related (0.75, 1.5 Hz, marked with red asterisks), triple-related (0.5, 1 Hz, marked with blue asterisks), and the beat frequency (3 Hz). Here, the duple-trained model produced larger responses at duple-related frequencies (0.75, 1.5 Hz) relative to the other models, while the triple-trained models produced larger responses at triple-related frequencies (0.5, 1 Hz) relative to the other models, suggesting that simultaneous auditory-vestibular training enhanced oscillatory responses to musical rhythm specifically at frequencies (i.e., harmonic and subharmonic frequencies) related to the rate of vestibular input.

Auditory-Vestibular Training Facilitates Neural Plasticity

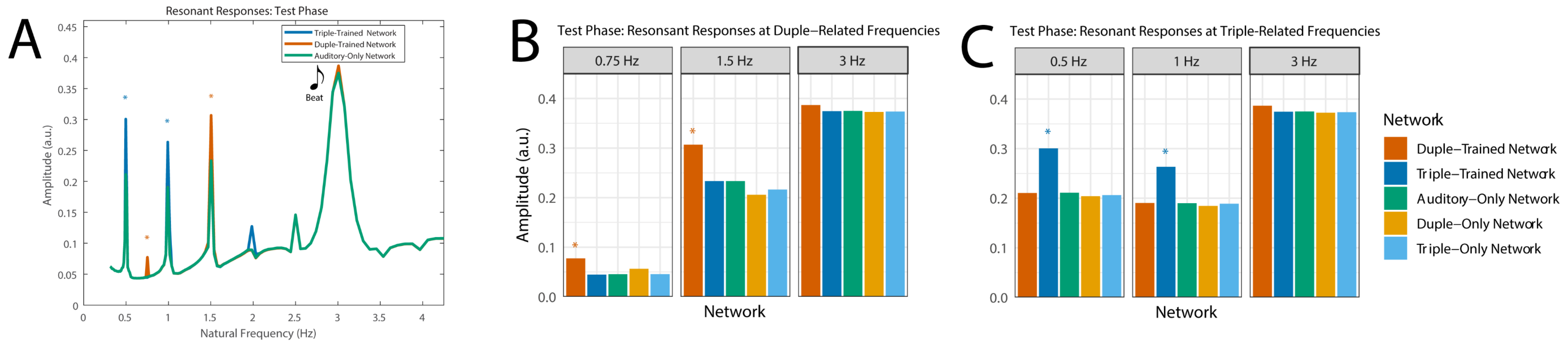


(A) Connection matrix of the duple-trained model. The duple-trained model, which was trained on an unaccented rhythm and duple-rate vestibular input, learned strong, bi-directional connections between 1.5 – 3 Hz, reflecting its rate of bouncing (1.5 Hz) and the beat level (3 Hz) of the rhythm.

(B) Connection matrix of the triple-trained model. The triple-trained model, a model trained on an unaccented rhythm and triple-rate vestibular input, exhibited more distributed learning, with bi-directional connections emerging between 0.5 – 1 Hz and 1 – 3 Hz, reflecting its rate of bouncing (1 Hz) and the beat and measure level (3 Hz, 0.5 Hz, respectively) of the rhythm.

(C) The time-course of learning oscillator connections at the strongest duple-related frequencies (1.5 – 3 Hz) and triple-related frequencies (0.5 – 1 Hz). **(C, Left)** The duple-trained network learned the strongest synaptic connection between network oscillators at 1.5 and 3 Hz, across all models. **(C, Right)** The triple-trained network learned the strongest synaptic connection between network oscillators at 0.5 and 1 Hz, relative to all models.

Auditory-Vestibular Models Preferred Vestibular-Related Rhythmic Frequencies



(A) Resonant responses (i.e., average oscillatory activity) for the duple-trained (red), triple-trained (blue), and auditory-only (green) models during the final half of the test procedure. Here, the duple- and triple-trained models resonated strongly at frequencies related to their vestibular training in response to the unaccented rhythm, suggesting that the models preferred rhythmic frequencies related to their bouncing.

(B) Resonant-response amplitude values for all models for duple-related frequencies during the test phase. Here, the duple-trained model produced the largest resonant responses at duple-related frequencies (0.75, 1.5 Hz; red asterisks) in response to the unaccented rhythm during the test phase, suggesting that the duple-trained model preferred rhythmic frequencies related to its bouncing.

(C) Resonant-response amplitude values for all models for triple-related frequencies during the test phase. Here, the triple-trained model produced the largest resonant responses at triple-related frequencies (0.5, 1 Hz; blue asterisks) in response to the unaccented rhythm during the test phase, suggesting that the triple-trained model preferred rhythmic frequencies related to its bouncing.

Summary and Interpretations

- Auditory-vestibular training shaped the neural response to musical rhythm, enhancing oscillatory activity at vestibular-related frequencies.
- Auditory-vestibular training facilitated neural plasticity, producing stronger connections between oscillators that embodied the structure of auditory-vestibular inputs.
- Auditory-vestibular training engendered a preference in the model for vestibular-related rhythmic frequencies:
  - Similar to infants' preference for accented rhythms that matched the rate of maternal bouncing (Phillips-Silver & Trainor, 2005).

Future Directions

- Towards a general framework of rhythm development using Neural Resonance Theory[4,5].
  - Model the effects of short- and long-term training on rhythm perception-action[6]
  - Model tempo preferences across the lifespan[7]
  - Implement multiple timescales of learning into the model

References

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Model Equations

$$\tau_{1i}\dot{z}_{1i} = \underbrace{z_{1i}\left(\alpha + i2\pi + \beta_1|z_{1i}|^2 + \frac{\beta_2|z_{1i}|^4}{1-|z_{1i}|^2}\right)}_{\text{Intrinsic Dynamics}} + \underbrace{x(t) + \sum_{j\neq i} c_{ij} z_{1j}^{k_{ij}} \bar{z}_{1i}^{m_{ij}-1} + \sum_j d_{ij}\frac{z_{2j}}{1-z_{2j}}\cdot\frac{1}{1-\bar{z}_{2j}}\cdot\frac{1}{1-\bar{z}_{1i}}}_{\text{Time-Varying Input and Oscillator Connections}} \quad (1a)$$

$$\tau_{2i}\dot{z}_{2i} = z_{2i}\left(\alpha + i2\pi + \beta_1|z_{2i}|^2 + \frac{\beta_2|z_{2i}|^4}{1-|z_{2i}|^2}\right) + y(t) \quad (1b)$$

Equations (1a, 1b) describe the dynamics of neural oscillators in the auditory (1a) and motor networks (1b). Here, z_{1i} and z_{2i} are complex-valued state variables whose real part represents the excitatory activity and whose imaginary part represents the inhibitory activity of the i^{th} neural oscillator in the auditory network, 1, and motor network, 2, respectively. The natural frequencies of the i^{th} oscillator in the auditory network, 1, and motor network, 2, is given by $f_{1i} = 1/\tau_{1i}$ and $f_{2i} = 1/\tau_{2i}$, respectively. When $\beta_1 < 0$, the endogenous activity of network oscillators is governed by the α parameter, where $\alpha_c = 0$ is the critical point. For $\alpha < 0$, the network oscillators will exhibit damped oscillation, while for $\alpha > 0$, the network oscillators will spontaneously oscillate via an Andronov-Hopf bifurcation. The βs reflect nonlinear damping parameters. Finally, c_{ij} represents input from the synaptic connection between the *j*th oscillator to the *i*th oscillator in the auditory network that are in a mode-locked relationship (i.e., *k:m* integer-ratio relationships), while d_{ij} represents oscillatory input from efferent connections that connect the motor network to the auditory network. *x(t)* and *y(t)* are time-varying inputs to the auditory and motor network, which reflect a musical rhythm and maternal bouncing, respectively.

$$\tau\dot{c}_{ij} = \underbrace{c_{ij}\left(\lambda_1 + \mu_1|c_{ij}|^2 + \frac{\epsilon_c\mu_2|c_{ij}|^4}{1-\epsilon_c|c_{ij}|^2}\right) + \kappa\sqrt{\epsilon_c}^{\,k_{ij}+m_{ij}-2} z_i^{m_{ij}} \bar{z}_j^{k_{ij}}}_{\text{Hebbian Learning Dynamics Between Mode-Locked Oscillators}} \quad (2)$$

Equation (2) describes the dynamics of Hebbian learning in the auditory network of the model. Here, c_{ij} is a complex variable that represents the amplitude and phase of the synaptic connection between the *j*th and *i*th oscillator in the auditory network. The parameters λ, $\mu1$, $\mu2$, κ, and ϵ_c determine the dynamics of the plasticity for oscillators that are near resonant frequency relationships, $m_{ij}f_i = k_{ij}f_i$. The unsubscripted t represents the global learning timescale. We set t to a small value (i.e., faster timescale) to simulate short-term plasticity thought to arise from auditory-vestibular training.